

*query language, data stream processing,
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DATA STREAM PROCESSING IN FETAL MONITORING SYSTEM: II. APPLICATION TO SIGNAL PROCESSING

Fetal monitoring system belongs to signal processing system class. The main functions of the system are signal acquisition from bedside monitors, on-line trace analysis and dynamic presentation of incoming data. Collected data set is controlled by centralised application. Relational database management system cannot process samples of high frequency biomedical signals on-line. Therefore, we decide to build our own data management system dedicated to stream processing that support continuous query. This paper describes a method of building a query plan based on proposed algebra. The presented example of application enables implementation of algorithm determining long- and short-term indices for fetal heart rate variability assessment on the basis of declarative query language. Our solution enables to define query based on data streams that make the updated answers currently available.

1. INTRODUCTION

Centralised fetal monitoring system is noticed as a signal processing system. This system was under development in our Institute since many years – now is available as a commercial unit called MONAKO [1,2]. The main functions of the system are signal acquisition from bedside monitors, on-line trace analysis and dynamic presentation of incoming data. All biomedical signals have controlled by centralised application and stored in append-only disk files. Signals are combined into uniform data stream. System alerts clinical services when any abnormal signals are detected.

Classical signals processing assumes that each part of the signal can be present in time window. Procedural high-level languages realise data processing. Source and computed data are stored finally in static objects (i.e. disk files). The main disadvantage of this approach is extremely complicated signal processing algorithm. Minor disadvantages are: available resources are not controlled, system architecture is not scaled easily and recorded data are not useable for second party applications. These problems solve application of specialised data management system.

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The specific character of recorded data determines the selection of an appropriate database management system. There are unavailable commercial database management systems well suited for signal processing. Relational database management system cannot process on-line high frequency biomedical signal's samples. Additionally relational systems have limited possibilities of fast recording data in large quantities. Therefore, we decide to build our own data management system dedicated to stream processing that support continuous queries [3]. Our goal is to develop flexible and more efficient solution – declarative query language for signal processing. Recorded data should be controlled by database management system, easy available for other systems. New, simpler algorithms will appear. System resources should be controlled by database management system.

The bases of our research are stream processing issues [4]. The data stream is an unbounded bag of elements (a,t) where the first element contains measured value and the second – time of occurrence. Most of all collected data by MONAKO are in form of time series – e.g. uniform data stream. Developed algebra and query language will help us simplify record of signal processing algorithms. Presented solutions are not able to perform signal processing required in present-day biomedical applications [5,6]. Declarative query language for signal processing needs specific operators. For instance, relational full join operator is useless considering its realisation time. Therefore, our conception is near to reduce instructions set in query language.

Created queries must return continuously updated answers. This kind of query is call continuous query. We have decided to build our own data management system dedicated to signal processing that support continuous query. Ongoing research on stream management system has not provided any sufficient and universal solutions so far. The main method of stream and signal computation is sliding window technique. It is a commonly used way of presenting selected part of the data stream and signal in time [7,8]. This paper describes a method of building a query plan based on the proposed algebra. The presented example of application enables implementation of algorithm determining long- and short-term indices for fetal heart rate variability assessment based on declarative query language.

2. DATA STREAM AND CONTINUOUS QUERY LANGUAGE

A stream can be considered as a set (multiset to be precise) of pairs (s,t) , indicating that a tuple arrives on the stream at time t i.e. the first element contains measured value and the second – time of its occurrence. In the MONAKO system the biomedical data streams can be presented in the form of time series. Time series are in the form of a bag of elements $(\{a_n\},\Delta)$, where the first element is data sequence and the second is a real number that determines time interval between the consecutive elements of the sequence. Every time series can be described with the help of data stream, however both definitions are not equivalent to each other. We found additionally for now, that input order is assumed and hold by recording system. Streams have the notion of an input order, they are unbounded, and they are append-only. By data stream schema A we will understand the list of attributes of individual elements (tuples) of sequence $\{a_n\}$. The schema is written in the following way $A(A_1,A_2,A_3)$, where A_1, A_2, A_3 represent areas the data are stored. It has to be noted that the relation of order within the list is compulsory. The order presented in the schema is binding. Considering data stream A as a bag of elements $(\{a_n\},\Delta_a)$ and assuming that all the

operations realised in database management system will refer to set of data streams, we determined the following set of operations necessary to implement the analytical procedures in MONAKO system: Interlace, Deinterlace, Sum, Difference, Aggregation/Serialisation, Projection and Selection (see Table 1).

Tab.1. Algebraic operations

Operation name	Algebraic notation
Interlace	$C := A\#B$
Deinterlace	$A := C\&\Delta b;B$
Sum	$C := A+B$
Difference	$A := C-(\Delta_a, \Delta_b)$
Aggregation/Serialisation	$B := AGSE(A, (A1, A2, \dots), step)$
Projection	$A' := A(A1, A2, \dots, An) \Rightarrow (A1, A2, \dots, Am)$
Selection	$C := A(A1, A2, \dots, An), X\Theta Y$

Presented set and operators state the base of Algebra. Some of them are analogous to operators presented in Aurora query algebra [6]. The current draft design of our query language is presented in Table II. Syntactically, our query language is based on SQL but disallowing the WHERE clause. All presented operations including window specification applied by AGSE operation are described in previous part of this paper.

Tab.2 Operations and example notations in continuous Query Language

Operation	Example in continuous query language
Interlace	SELECT a, b AS C FROM A#B
Deinterlace	SELECT a AS A FROM C&2
Sum	SELECT a, b AS C FROM A+B
Difference	SELECT a AS A FROM C-(1, 2)
Aggregation/Serialisation	SELECT AGSE(C, NUMBER<10>, 1) FROM C
Projection	SELECT a FROM C
Selection	SELECT a FROM C FILTER C BY a>10

As example we present construction of query plan based on presented assumptions. In Relational DBMSs, all operators are pull-based: an operator requests data from the plan only when needed. In contrast, stream operators consume data pushed to the system by the external devices. Operators should be scheduled in order to minimise queue size and queuing delays. Another problem is continuous query plan based on actual and retrospective data.

3. APPLICATION

One of the most important features of physiological FHR trace is that the intervals between fetal heartbeats permanently undergo the small changes. Changes of the duration of successive cardiac cycles are determined as short-term variability (STV). The changes of STV direction and

value, causing an FHR oscillation in relation to its mean value, are denoting as long-term variability (LTV). In a real FHR trace, both types of variability coexist showing the mutual relationship. In order to assess these values, the variability indices have introduced. Procedure of the index computation is performing in buffers. The computation of each index occurs every minute and requires the collection of 240 FHR signal samples. Since the indices are defined on a basis of signal averaged over 2.5 s periods, their presampling is necessary. To this end, the samples are group in tens, and for each group the mean value is determined thus creating the *Fhr_Avg* table, which is a common basis for further determination of LTV and STV indices. When determining the STV, *Fhr_DivAvgMonitor* table is creating containing the differences between successive elements of *Fhr_Avg* table. STV value, placed in the window with results of analysis, presents a mean value from all elements of the *Fhr_DivAvgMonitor* table. To compute LTV there are determined the minimal and maximal elements within *Fhr_Avg* table, whereas the resulting LTV demonstrates the difference between these values. Consecutive LTV and STV values create a sequence of currently added values. These values are present together with FHR signal in a form of histograms including the averaged information on changes in a fetal heart rhythm. The diagram updates every minute.

MONAKO system records input stream (*InStream*) from 8 bedside fetal monitors. Elements of this stream are added every 0.125 seconds. Every tuple contains information about monitor number and values of measured signals: fetal heart rate (FHR), oxygen saturation (OXY), and uterine contraction (UC). Our goal is to present the sequence of necessary operations (query plan) with the help of previously defined operations, enabling calculation so-called long- and short-term FHR variability indices (LTV and STV) presented in MONAKO system for the monitor number 1. Data stream interval Δ in MONAKO system is nominated by a unit of time calculated in seconds. Input stream schema *InStream*, 0.125s (1) is presented as follows:

$$InStream (ID_FMonitor, FHR_1, FHR_2, FHR_3, FHR_4, OXY, UC) \quad (1)$$

First operation is selection of tuples belonging to fetal monitor number 1. This operation is recorded in the following way (2):

$$FMonitor1 := InStream (ID_FMonitor, FHR_1, FHR_2, FHR_3, FHR_4, OXY, UC), ID_FMonitor = 1 \quad (2)$$

Resulting stream contains tuples coming exclusively from the monitor number 1. The interval Δ of the resulting stream is 1s. Deinterlace operation of the given streams for this data stream cannot be applied. We have to take into consideration the input stream including data from only few fetal monitors that can be connected. This way we receive data stream *FMonitor1*, 1s (2) whose consecutive tuples are added once in every second. Next operation is the projection operation:

$$\begin{aligned} FHR4_FMonitor1 &:= FMonitor1 (ID_FMonitor, FHR1, FHR2, FHR3, FHR4, OXY) \\ &=> (FHR1, FHR2, FHR3, FHR4) \end{aligned} \quad (3)$$

Interval Δ remains unchanged and equals 1s (3). Next step is serialisation (4) operation of stream *FHR4_FMonitor1*, 1s (3).

$$FHR_FMonitor1 := FHR4_FMonitor1 (DOM(FHR), 1) \quad (4)$$

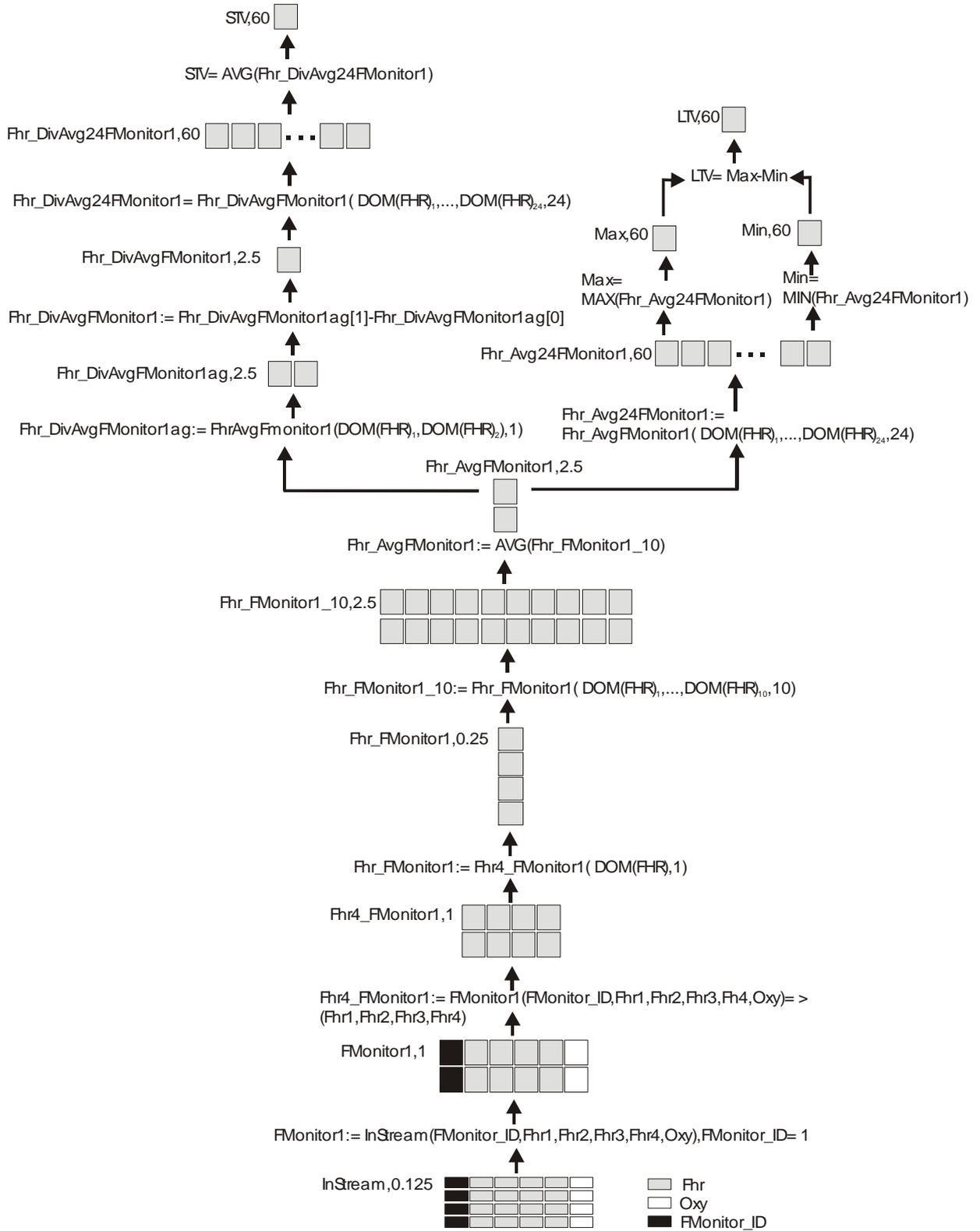


Fig.1 Query plan for STV and LTV index computation.

After this operation has been finished we receive data stream $FHR_FMonitor1, 0.25s$ (4). Notation $DOM(FHR)$ means domain of FHR, i.e. in our example $DOM(FHR)$ means NUMBER. Its elements contain atomic, measured values of fetal heart rate (FHR). 240 samples of consecutive values of fetal heart rate are required to determine long- and short-term variability indices.

Because variability indices are defined on the basis of average signal for the period of 2.5 seconds, it is necessary to sample it. Considering this, samples are grouped in 10s. An average value is determined from every appointed group. The created table of 24 values is the direct base to determine the searched indices. The described process of determining indices should be started from data streams aggregation $FHR_FMonitor1, 0.25s$ (4).

$$FHR_FMonitor1_10 := FHR_FMonitor1 ((DOM(FHR)_1, \dots, DOM(FHR)_{10}), 10). \quad (5)$$

$DOM(FHR)_1, \dots, DOM(FHR)_{10}$ record means data schema consisted of 10 fields including consecutive values of FHR. Every stream tuple $FHR_FMonitor1_10, 2.5s$ (5) includes data from 10 recorded by the monitor measurements of fetal heart rate values e.g. $(FHR(n+1), FHR(n+2), \dots, FHR(n+10))$. As a result of algebraic simplification it is feasible to link two previous operations in one (6).

$$FHR_FMonitor1_10 := FHR4_FMonitor1 ((DOM(FHR)_1, \dots, DOM(FHR)_{10}), 4) \quad (6)$$

For further calculation it is necessary to create stream including average from determined tuples – with this end in view we carry out the following operation:

$$FHR_AvgFMonitor1 := AVG (FHR_FMonitor1_10) \quad (7)$$

Stream whose schema is as follows is created: $FHR_AvgFMonitor1 (DOM(FHR))$, its elements are added once in every 2,5 seconds (7). Every following stream tuple $FHR_AvgFMonitor1, 2.5s$ (7) includes information about average from 10 consecutive measured FHR values. Short-term variability index (STV) is determined on the basis of 24 consecutive elements of the stream, whose tuples store the difference of consecutive elements of the stream $FHR_AvgFMonitor1, 2.5s$ (7). The following operations enable to create the stream whose consecutive elements present differences of consecutive elements of the stream $FHR_AvgFMonitor1, 2.5s$ (8).

$$FHR_DivAvgFMonitor1ag := FHR_AvgFMonitor1 ((DOM(FHR)_1, DOM(FHR)_2), 1)$$

$$FHR_DivAvgFMonitor1 := FHR_DivAvgFMonitor1ag.FHR2 \quad (8)$$

$$- FHR_DivAvgFMonitor1ag.FHR1$$

The stream schema $FHR_DivAvgFMonitor1, 2.5s$ is identical with schema $FHR_AvgFMonitor1, 2.5s$ (8). Determination of short-term variability index requires calculation of the average from consecutive 24 elements of stream $FHR_DivAvgFMonitor1, 2.5s$ (8). The next

step is the calculation of the average from every received tuple. First operation can be realised by stream aggregation $FHR_DivAvgFMonitor1$, 2.5s.

$$FHR_DivAvg24FMonitor1 := FHR_DivAvgFMonitor1 (DOM(FHR)1, \dots, DOM(FHR)24, 24) \quad (9)$$

As a result of aggregation the stream is created $FHR_DivAvg24FMonitor1$, 60s (9) including 24 elements in every tuple. The function determining the average occurs in the second operation.

$$STV_FMonitor1 := AVG(FHR_DivAvg24FMonitor1) \quad (10)$$

After these operations have been finished the stream $STV_FMonitor1$ s, 60s (10) includes consecutive determined short-term variability index. Consecutive elements to this stream are added once in every minute – so the interval Δ equals 60s.

Long term variability index LTV is determined on the basis of stream $FHR_Avg24FMonitor1$, 2.5s (9). In order to determine this index it is necessary to create data stream whose elements will contain the difference between minimal and maximal value of stream elements $FHR_Avg24FMonitor1$, 2.5s (9). Formal record of this operation looks as follows:

$$LTV_FMonitor1 := MAX(FHR_Avg24FMonitor1) - MIN(FHR_Avg24FMonitor1) \quad (11)$$

Stream $LTV_FMonitor1$, 60s (11) and $STV_FMonitor1$, 60s (10) presented this way include determined consecutive long- and short-term variability indices for given data recorded by MONAKO system. Realisation plan (Fig.1) will be feasible to create in declarative query language on the basis of the following continuous queries:

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select AVG(AGSE((FHR_AvgFMonitor1[1]-FHR_AvgFMonitor1[0]),NUMBER<24>,24))
as STV_FMonitor1 from
    select AGSE( AVG( AGSE((FHR1,FHR2,FHR3,FHR4),NUMBER<10>,4) ),NUMBER<2>,1)
    as FHR_AvgFMonitor1 from InStream
    Filter InStream By ID_FMonitor = 1

select AVG( MAX(FHR_Avg24FMonitor1)-MIN(FHR_Avg24FMonitor1))
as LTV_FMonitor1 from
    select aGSE(AVG(AGSE((FHR1,FHR2,FHR3,FHR4),NUMBER<10>,4) ),NUMBER<24>,24)
    as FHR_Avg24FMonitor1 from InStream
    Filter InStream By ID_FMonitor = 1
    
```

4. CONCLUSIONS

Database management systems are not efficient enough in biomedical applications. Pending research on query languages based on data streams results creating some new concepts - including ours. Stream Algebra and continuous declarative query language are the basis of the designed data stream management system. Access to the recorded biomedical signals will be realised by the presented query language. The presented example of application enables implementation of

algorithm determining long- and short-term variability indices LTV and STV on the basis of declarative query language. The system realising the techniques described in this paper is being developed at Institute of Medical Technology and Equipment.

Our solution enables to define query based on data streams that make the updated answers currently available. In contrast to presented so far solutions, we do not enable – at present – linking of the recorded in data streams information with the information stored in relational database. It is also worth noting that in the presented declarative query language the WHERE clause does not occur. Similar but very limited function is played by the FILTER BY clause intended exclusively to determine the conditions of data filtering. Presented declarative query language required drawing up and presenting assumptions of data algebra intended to analyses and record of biomedical signals. The ongoing researches are carried out in the framework on MONAKO system project. At the present time its architecture is centralised. However, applying database management system that carries out its tasks on the basis of presented assumptions enables the construction of monitoring system of distributed architecture.

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